

Multiple Kernel Learning in the Primal for Multimodal Alzheimer's Disease Classification

Fayao Liu, Luping Zhou, Chunhua Shen, and Jianping Yin

Abstract—To achieve effective and efficient detection of Alzheimer's disease (AD), many machine learning methods have been introduced into this realm. However, the general case of limited training samples, as well as different feature representations typically makes this problem challenging. In this paper, we propose a novel multiple kernel-learning framework to combine multimodal features for AD classification, which is scalable and easy to implement. Contrary to the usual way of solving the problem in the dual, we look at the optimization from a new perspective. By conducting Fourier transform on the Gaussian kernel, we explicitly compute the mapping function, which leads to a more straightforward solution of the problem in the primal. Furthermore, we impose the mixed L_{21} norm constraint on the kernel weights, known as the group lasso regularization, to enforce group sparsity among different feature modalities. This actually acts as a role of feature modality selection, while at the same time exploiting complementary information among different kernels. Therefore, it is able to extract the most discriminative features for classification. Experiments on the ADNI dataset demonstrate the effectiveness of the proposed method.

Index Terms—Alzheimer's disease (AD), group Lasso, multimodal features, multiple kernel learning (MKL), random Fourier feature (RFF).

I. INTRODUCTION

AS the most common type of dementia among the elders, Alzheimer's disease (AD) is now affecting millions of people over the world. It is characterized by progressive brain disorder that damages brain cells, leading to memory loss, confusion, and eventually to death. The huge price of caring AD patients has made it one of the most costly diseases in many developed countries, and also caused great physical, as well as psychological burdens on the caregivers. From this perspective, early diagnosis of AD can be of great significance. Identified in an early stage, the disease can be made well under control.

Previous diagnosis mainly depends on evaluation of the patient history, clinical observation, or cognitive assessment.

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Recent AD-related research showed promising prospect in finding reliable biomarkers for automatic early detection [1], which is a promising yet challenging task. Many projects such as Alzheimer disease neuroimaging initiative (ADNI) [2] have been launched to collect data of candidate biomarkers to promote the development of AD research. Several biomarkers have been studied and proved to be sensitive to mild cognitive impairment (MCI)—an early stage of AD, e.g., brain atrophy detected by imaging [3], protein changes in blood or spinal fluid [4], genetic variations (mutations) [5], etc. With accurate early diagnosis of MCI, the progression of converting to AD can be possibly slowed down and well controlled.

Recent studies [6], [7] indicate that image analysis of brain scans is more reliable and sensitive in detecting the presence of early AD than traditional cognitive evaluation. In this context, many machine-learning methods have been introduced to perform neuroimaging analysis for automatic AD classification. Early attempts mainly focused on applying off-the-shelf tools in statistical machine learning to differentiate AD, with the most popular one being support vector machines (SVMs).

Klöppel *et al.* [8] trained a linear SVM to classify AD patients and cognitively normal individuals using magnetic resonance imaging (MRI) scans. More SVM-based approaches can be found in [9] and [10]. Besides SVMs, other learning methods are also introduced. Tripoliti *et al.* [7] applied Random Forests on functional MRI (fMRI) obtained from 41 subjects to differentiate AD and health control. In [6], Casanova *et al.* implemented a penalized logistic regression to classify sMRI images of cognitive normal subjects and AD patients from ADNI datasets. Note that they all used single feature modality for classification.

However, as indicated by [4], different biomarkers may carry complementary information. Therefore, combining multimodal features, instead of depending on one feature alone is a promising direction for improving classification accuracy. Intuitively, one can combine multiple results from different classifiers with voting techniques or ensemble methods. Dai *et al.* [11] proposed a multiclassifier fusion model through weighted voting, using maximum uncertainty linear discriminant analysis as base classifiers, to distinguish AD patients and healthy control (HC). They used features from both sMRI and fMRI images. Polikar *et al.* [12] proposed an ensemble method based on multilayer perceptron to combine electroencephalography, positron emission tomography (PET), and MRI data. A linear program boosting algorithm was used by Hinrichs [13] to jointly consider features from MRI and fluorodeoxyglucose PET.

Moreover, concatenating several features into one single vector and then training a classifier can also be a practical option. Walhovd *et al.* [14] performed logistic regression

analysis by concatenating MRI, PET, and cerebrospinal fluid (CSF) features. However, such concatenation requires proper normalization of features extracted from different sources. Otherwise the prediction score would be easily dominated by a single feature. Another disadvantage of this method is that it treats multiple features equally, being incapable of effectively exploring the complementary information provided by different feature modalities.

In addition to the aforementioned fusion approaches, another method is multiple kernel learning (MKL) [15], [16], which works by simultaneously learning the predictor parameters and the kernel combination weights. The multiple kernels can come from different sources of feature spaces, thus providing a general framework for data fusion. It has found successful applications in genomic data fusion [15], protein function prediction [17], etc. As for AD data fusion and classification, Hinrichs *et al.* [18] proposed an MKL method, which casts each feature as one or more kernels and then solves for support vectors and kernel weights using simplex constraints, known as SimpleMKL [19]. Cuingnet *et al.* [20] evaluated ten methods for predicting AD, including linear SVM, Gaussian SVM, logistic regression, MKL, etc., also based on SimpleMKL. More recently, Zhang *et al.* [21] proposed an SVM-based model to combine kernels from MRI, PET, and CSF features. Their formulation does not involve kernel coefficients learning. Instead, they use grid search to find kernel weights, which can be very time consuming or even intractable when the number of kernels or features is large. It is worth noting that they all solve the MKL problem in the Lagrange dual space. Therefore, the time complexity scales at least $O(n^{2.3})$ [22] with respect to the size n of the training set.

Here, we propose to directly solve the primal MKL problem. This is achieved by explicitly computing the mapping functions through Fourier extension of the kernel functions, inspired by the random features proposed by Rahimi and Recht [23]. By sampling components from the Fourier space of the Gaussian kernel using Monte Carlo methods, we can obtain an approximate embedding, and hence reduce the complexity of the kernel learning problem to $O(n)$. Furthermore, instead of the most commonly used L_1 , L_2 norm, we impose the mixed L_{21} norm constraint on the kernel weights, known as the group Lasso, to enhance group sparsity among different feature modalities. In summary, we highlight the main contributions of this paper as follows:

- 1) We use random Fourier features (RFFs) to approximate Gaussian kernels, leading to the simple primal solution of the MKL problem. Therefore, the learning complexity is reduced to linear scale in the number of the training data.
- 2) We enforce an L_{21} norm constraint on the kernel weights, to promote group sparsity among different feature modalities, while simultaneously exploiting the complementary information among different kernels. It can be used to select the most discriminative features to improve classification accuracy.
- 3) The proposed RFF + L_{21} norm MKL framework is used to perform feature selection on regions of interest (ROI) features of AD datasets, therefore identifying brain regions that are most related to AD. The proposed method yields a

simple primal solution and provides a general framework for heterogeneous feature integration.

The rest of this paper is organized as follows. In Section II, we first briefly review some preliminaries of SVMs and MKL, and then present our formulation and the detailed algorithm. Experimental results are reported and discussed in Section III, and conclusions are made in Section IV.

II. METHODS

Before presenting the details of the method, we first define some notation. A column vector is denoted by a bold lower-case letter (\mathbf{x}) and a matrix is represented by a bold upper-case letter (\mathbf{X}). $\xi \succeq \mathbf{0}$ indicates all elements of ξ being non-negative.

A. MKL Revisit

SVMs [24] is a large margin method, based on the theory of structural risk minimization. In case of binary classification, SVMs finds a linear decision boundary that best separates the two classes. When it comes to nonlinear separable cases, a mapping function $\Phi: \mathbb{R}^d \rightarrow \mathbb{R}^{d'}$ ($d' > d$) is adopted to embed the original data into a higher dimensional space, finally yields linear decision boundary $f(\mathbf{x}) = \mathbf{w}^T \Phi(\mathbf{x}) + b$. Given a labeled training set $\{(\mathbf{x}_i, y_i)\}_{i=1}^n$, where $\mathbf{x}_i \in \mathbb{R}^d$ denotes the training sample and $y_i \in \{-1, +1\}$ the corresponding class label, canonical SVM solves the following problem:

$$\begin{aligned} \min_{\mathbf{w}, b} \quad & \frac{1}{2} \|\mathbf{w}\|^2 + C \sum_i \xi_i \\ \text{s.t.} \quad & y_i (\langle \mathbf{w}, \Phi(\mathbf{x}_i) \rangle + b) \geq 1 - \xi_i, \forall i \\ & \xi \succeq \mathbf{0} \end{aligned} \quad (1)$$

where C is a tradeoff parameter between training error and margin maximization, $\xi = [\xi_1, \dots, \xi_n]^T$ the slack variables, and $\langle \cdot, \cdot \rangle$ represents inner product. While finding the appropriate mapping function Φ is always difficult, one usually resorts to solving it in the Lagrange dual space by the kernel trick

$$k(\mathbf{x}, \mathbf{x}_i) = \langle \Phi(\mathbf{x}), \Phi(\mathbf{x}_i) \rangle. \quad (2)$$

As Φ only appears in inner product form, by such a simple substitution, one can instead solve the following Lagrange dual problem (3) without explicitly knowing the embedding Φ :

$$\begin{aligned} \max_{\alpha} \quad & \sum_i \alpha_i - \frac{1}{2} \sum_{i,j} \alpha_i \alpha_j y_i y_j k(\mathbf{x}_i, \mathbf{x}_j) \\ \text{s.t.} \quad & 0 \leq \alpha_i \leq C, \forall i, \sum_i \alpha_i y_i = 0 \end{aligned} \quad (3)$$

where α_i are Lagrange multipliers, and k the kernel, which is typically predefined. Several frequently involved kernels are linear, polynomial, Gaussian, sigmoid kernel, etc.

To this end, the algorithm performance relies largely on the kernel one chooses. While finding the appropriate kernel may not be straightforward, many researchers turned to using multiple kernels instead of a single one and tried to find the optimum combination of them. The different kernels may correspond to different similarity representations or different feature sources.

A simple option is to consider the convex combination of basic kernels

$$k(\mathbf{x}_i, \mathbf{x}_j) = \sum_m \beta_m k_m(\mathbf{x}_i, \mathbf{x}_j) \quad (4)$$

with $\sum_m \beta_m = 1, \beta \succeq \mathbf{0}$, where β_m denotes the weight of the m th kernel function.

The process of learning the kernel weights while simultaneously minimizing the structural risk is known as the MKL. As one of the state-of-the-art MKL algorithms, SimpleMKL [19] efficiently solves a simplex constrained MKL formulation. The primal MKL problem with L_1 norm constraint is formulated as

$$\begin{aligned} \min_{\mathbf{w}, \beta, \xi} \quad & \frac{1}{2} \sum_m \frac{1}{\beta_m} \|\mathbf{w}_m\|_2^2 + C \sum_i \xi_i \\ \text{s.t.} \quad & y_i \left(\mathbf{w}^T \sum_l \Phi_l(\mathbf{x}_i) + b \right) \geq 1 - \xi_i, \forall i \\ & \sum_m \beta_m = 1, \beta \succeq \mathbf{0}, \xi \succeq \mathbf{0}. \end{aligned} \quad (5)$$

While the L_1 norm is known as a sparsity inducing norm, one can easily replace the simplex constraint $\sum_m \beta_m = 1$ with the ball constraint $\sum_m \beta_m^2 \leq 1$, which usually yields the nonsparse solution. Again, the mapping Φ is conducted implicitly, which draws its corresponding Lagrange dual problem into spotlight

$$\begin{aligned} \min_{\beta} \max_{\alpha} \quad & \sum_i \alpha_i - \frac{1}{2} \sum_{i,j} \alpha_i \alpha_j y_i y_j \sum_m \beta_m k_m(\mathbf{x}_i, \mathbf{x}_j) \\ \text{s.t.} \quad & \sum_i \alpha_i y_i = 0 \\ & 0 \leq \alpha_i \leq C, \forall i, \sum_m \beta_m = 1, \beta \succeq \mathbf{0} \end{aligned} \quad (6)$$

where α_i, α_j are Lagrange multipliers and $k_m(\mathbf{x}_i, \mathbf{x}_j)$ is the m th kernel function.

B. Proposed MKL for Combining Multimodal Features

MKL provides a principled way of incorporating multimodal features by using multiple kernels. However, due to the unknown mapping Φ , they usually must be solved in the Lagrange dual space, which results in a time complexity of at least $O(n^{2.3})$ [22] with respect to the data size n . We thus seek to look at the MKL problem from a new perspective. Instead of solving it in the dual space, we propose to directly approximate the mapping function through Fourier transform of the kernels, leading to the primal solution of the problem. This is originally inspired from the random features proposed by Rahimi and Recht [23]. Specifically, we explicitly seek a $\Psi(\cdot)$ satisfying

$$k(\mathbf{x}_i, \mathbf{x}_j) \approx \langle \Psi(\mathbf{x}_i), \Psi(\mathbf{x}_j) \rangle. \quad (7)$$

Therefore, we can simply transform the primal data with Ψ and solve the primal MKL problem in the new feature space. In this section, we will first introduce the RFFs, and then give our formulation and the detailed algorithm.

1) *Random Fourier Features*: In order to approximate Φ , we conduct Fourier transform on kernel functions. Here, we

TABLE I
GAUSSIAN KERNEL AND ITS CORRESPONDING FOURIER TRANSFORM

kernel name	k(t)	p(ω)
Gaussian	$e^{-\frac{t^2}{2\sigma^2}}$	$\sqrt{2\pi}\sigma e^{-\frac{\omega^2\sigma^2}{2}}$

Algorithm 1 Compute random Fourier feature

Input: Matrix of training samples \mathbf{X} , Fourier size D , Gaussian kernel bandwidth σ

1. Compute Gaussian kernel matrix \mathbf{K} .
2. Compute the Fourier transform p of the kernel.
3. Draw D samples $\omega_1, \omega_2, \dots, \omega_D \in \mathbb{R}^d$ from p by Monte Carlo sampling.
4. $\Psi(\mathbf{X}) = \frac{1}{\sqrt{D}} [\cos(\omega'_1 \mathbf{X}), \dots, \cos(\omega'_D \mathbf{X}), \sin(\omega'_1 \mathbf{X}), \dots, \sin(\omega'_D \mathbf{X})]$

Output: $\Psi(\mathbf{X})$

adopt the most commonly used Gaussian kernel, whose Fourier transform [23] is illustrated in Table I. As can be seen from the table, the Fourier transform of a Gaussian function also conforms to a Gaussian distribution. Moreover, the bandwidth σ in time space corresponds to $\frac{1}{\sigma}$ in Fourier frequency space. Therefore, we can adopt random Fourier basis $\cos(\omega'x)$ and $\sin(\omega'x)$ to represent the random feature mapping Ψ , where $\omega \in \mathbb{R}^d$, are random variables drawn from frequency space of Gaussian kernel using Monte Carlo sampling.

The algorithm of computing random feature map Ψ can be described as Algorithm 1.

2) *Proposed MKL Framework*: Given p different feature groups, the samples are represented as $\mathbf{X} = \{(\mathbf{x}_i^{(1)}, \dots, \mathbf{x}_i^{(p)})\}_{i=1}^N$. For each feature group, we use q kernel functions to produce q embeddings. After explicitly computing the RFFs Ψ according to each kernel, we propose to solve the following primal objective function:

$$\begin{aligned} \min_{\mathbf{w}, \beta, \xi} \quad & \frac{1}{2} \sum_{l=1}^p \sum_{m=1}^q \frac{1}{\beta_{lm}} \|\mathbf{w}_{lm}\|_2^2 + C \sum_{i=1}^N \xi_i \\ \text{s.t.} \quad & y_i \left(\sum_{l=1}^p \sum_{m=1}^q \mathbf{w}_{lm}^T \Psi_{lm}(\mathbf{x}_i^{(l)}) + b \right) \geq 1 - \xi_i, \forall i \\ & \sum_{l=1}^p \|\beta_l\|_2 \leq 1, \beta \succeq \mathbf{0}, \xi \succeq \mathbf{0} \end{aligned} \quad (8)$$

where l indexes different feature groups and m indexes multiple kernels used for a single feature group. This is a convex optimization problem, which can be efficiently solved using off-the-shelf solvers like CVX [25] and MOSEK [26].

It is worth noting that we use the well-known group Lasso (L_{21} norm) constraint of the kernel weights instead of the commonly used L_1 norm. As according to Yan *et al.* [27], the L_1 norm is less effective when the combined kernels carry complementary information. While as stated previously, different biomarkers of AD may carry complementary knowledge, which serves as a reason why the L_1 norm underperforms other formulations, as indicated by experiments later. Instead, the mixed

Algorithm 2 Proposed MKL Algorithm

Input: Training samples $\{(\mathbf{x}_i^{(l)}, y_i)\}_{i=1}^N$, trade-off parameter C , Gaussian kernels \mathbf{K}_{l_m} , Fourier size D

1. **for** each kernel matrix \mathbf{K}_{l_m} **do**
 Compute Ψ_{l_m} by Alg. 1
2. Solve the primal MKL formulation (8)

Output: \mathbf{w}_{l_m}, b

L_{21} norm formulation enforces group sparsity among different feature modalities, which actually performs as a role of feature modality selection, while at the same time exploiting complementary information among the different kernels. Note that this group Lasso constraint has been widely used and proved to be of great success [28], [29]. To demonstrate the effectiveness of the proposed RFF + L_{21} norm framework, we also implemented the RFF + L_1 , RFF + L_2 norm formulation, simply by substituting the $\sum_l \|\beta_l\|_2 \leq 1$ constraint to $\|\beta\|_1 \leq 1$, $\|\beta\|_2 \leq 1$, respectively. The decision function thus can be written as

$$f(\mathbf{x}) = \text{sign} \left[\sum_{l=1}^p \sum_{m=1}^k \mathbf{w}_{l_m}^T \Psi_{l_m}(\mathbf{x}^{(l)}) + b \right]. \quad (9)$$

The overall framework is described in Algorithm 2.

III. RESULTS AND DISCUSSIONS

To evaluate the performance of the proposed MKL framework, we conduct experiments on the AD dataset obtained from ADNI [2]. The Fourier transform parameter D in our method is set to 2000, and a fivefold cross validation is conducted on the training set to optimize C (trying values 0.01, 0.1, 1, 10, 100). We use Gaussian kernels with ten different kernel bandwidths ($\{2^{-3}, 2^{-2}, \dots, 2^6\}$ multiplied by \sqrt{d} with d being the dimension of the feature) for each feature representation, which yields 40 kernels in total.

A. Subjects and Data Preprocessing

The AD dataset is composed of 120 subjects, randomly drawn from the ADNI database. It includes 70 HCs and 50 progressive MCI patients that developed probable AD after the baseline scanning.

Each subject is represented by a 229-dimensional feature, coming from two heterogeneous data sources: CSF biomarkers and MRI. We categorize the MRI feature into three groups, namely, left hemisphere hippocampus shape (HIPL), right hemisphere hippocampus shape (HIPR), and grey matter volumes within ROI, as they capture different aspects of information. We refer them (CSF, HIPL, HIPR, ROI) as four feature representations. For more details, the CSF biomarkers are provided by ADNI, including baseline CSF Ab (42), total tau (t-tau) and phosphorylated tau [p-tau (181)]. The hippocampal shapes are extracted from T1-weighted MRI and represented by spherical harmonics (SPHARM) for each hemisphere. To mitigate the influence of misalignment, a rotation-invariant SPHARM representation [30] is employed, which also reduces the dimensionality of the shape descriptors. The brain regional gray matter

TABLE II
FOUR FEATURE REPRESENTATIONS OF THE AD DATASET

Name	Dimension	Data Source	Representation
CSF	3	CSF	Cerebrospinal fluid
HIPL	63	MRI	Left hippocampus shape
HIPR	63	MRI	Right hippocampus shape
ROI	100	MRI	ROI volume

volumes are measured within 100 ROI via an ROI atlas [31] on tissue segmented brain images that have been spatially normalized into a template space [32] after intensity correction, skull stripping, and cerebellum removal.

We summarize the features in Table II. The CSF and ROI features are normalized to 0 means with unit variations.

B. AD Classification

To give an overall evaluation of the proposed method, in addition to the prediction accuracy (ACC), we use four indicators, namely, sensitivity (SEN), specificity (SPE), Matthews correlation coefficient (MCC) [33] and the area under the ROC curve (AUC).

We run the proposed algorithms 20 times on the AD dataset with randomly partitioned training and testing sets (2/3 for training and 1/3 for testing). The best accuracy results of SVM by using different kernels on each single feature representation and on the concatenated features [denoted as SVM (All)] are used as baselines. Table III reports the results of mean \pm std, with best scores highlighted in bold. As can be observed, among all the four types of features, ROI feature appears to be the most discriminative one, with an accuracy of 82.63%. Combining features from multiple modalities indeed outperforms the best single-feature-based classifier. Even a simple concatenation can improve the performance. As indicated by the MCC values, the proposed RFF + L_{21} formulation achieves the best overall performance, being slightly better than the SimpleMKL. The L_{21} norm turns out to be more effective than the L_1 , L_2 norm.

For further validation of the proposed method, we design an extra experiment to compare our framework with [21]. We implemented their method by exactly following the description in their paper. To be more precise, a coarse grid search through cross validation is adopted to find the optimal kernel weights and then an SVM is trained [solve (3)] by the selected kernel combination weights and linear kernels. The SVM is implemented by LIBSVM toolbox [34] with $C = 1$, as did in [21]. We use the same experimental settings as in [21]. Specifically, the whole dataset is equally partitioned into ten subsets, and each time one subset is chosen as test set and all the rest are for training. This process is repeated ten times for different partitions to ensure unbiased evaluation. For the implementation of [21], a tenfold cross validation is performed on the training data in each round to determine the optimal kernel weights β through a grid search ranging from 0 to 1 at a step size of 0.1. For our method and SimpleMKL, we also fix $C = 1$ and use the same kernel settings as above. Table IV shows the average performance.

According to Table IV, our method outperforms [21] and SimpleMKL in terms of all the four criteria. The reasons can be

TABLE III
COMPARISON OF PERFORMANCE USING SINGLE AND MULTI FEATURE REPRESENTATION CLASSIFICATION METHODS ON THE AD DATASET OVER 20 INDIVIDUAL RUNS

Method	ACC(%)	SEN(%)	SPE(%)	MCC(%)	AUC
SVM (CSF)	78.38 ± 5.58	80.30 ± 8.13	75.05 ± 9.53	55.43 ± 11.56	0.826 ± 0.064
SVM (HIPL)	77.75 ± 5.90	84.21 ± 7.38	69.61 ± 10.86	54.16 ± 12.19	0.844 ± 0.059
SVM (HIPR)	77.50 ± 6.49	81.53 ± 8.24	72.97 ± 13.10	54.30 ± 13.42	0.832 ± 0.069
SVM (ROI)	82.63 ± 5.10	94.02 ± 5.42	66.50 ± 7.24	64.58 ± 9.91	0.899 ± 0.040
SVM (All)	83.62 ± 6.10	93.91 ± 5.22	69.75 ± 9.41	66.87 ± 10.93	0.913 ± 0.034
SimpleMKL	85.88 ± 4.00	90.53 ± 6.73	79.47 ± 7.24	70.87 ± 8.13	0.934 ± 0.039
RFF+ L_1	83.12 ± 6.12	86.35 ± 7.98	78.29 ± 13.00	65.32 ± 13.10	0.905 ± 0.034
RFF+ L_2	85.12 ± 4.62	87.97 ± 6.92	80.83 ± 12.12	69.42 ± 9.90	0.921 ± 0.033
RFF+ L_{21}	87.12 ± 3.37	91.79 ± 5.08	80.73 ± 7.35	73.30 ± 7.37	0.952 ± 0.038

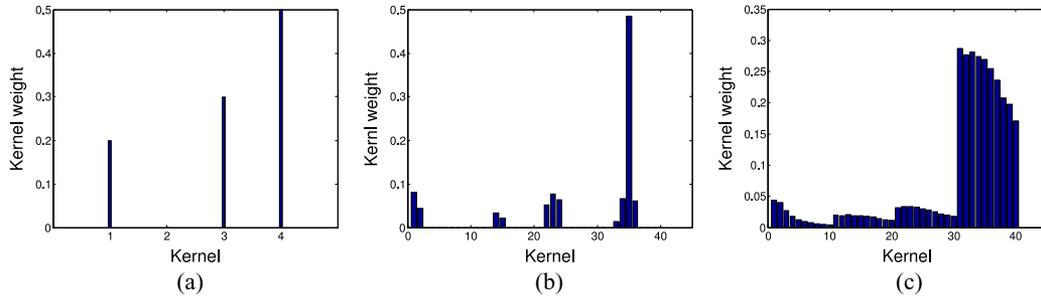


Fig. 1. Base kernel weights comparison of different MKL algorithms on the AD dataset. (a) [21]; (b) SimpleMKL; (c) Proposed RFF + L_{21} norm formulation. In (a), according to [21], only one linear kernel is used for each feature representation. In (b) and (c), from left to right, every ten kernels correspond to CSF, HIPL, HIPR, ROI, respectively.

TABLE IV
AVERAGE PERFORMANCE OF DIFFERENT METHODS ON THE AD DATASET

Method	ACC	SEN	SPE	MCC
[21]	86.39%	85.74%	86.93%	72.02%
SimpleMKL	87.06%	87.89%	86.68%	74.57%
RFF+ L_1	81.94%	83.83%	78.97%	63.31%
RFF+ L_2	85.00%	85.49%	84.28%	69.41%
RFF+ L_{21}	90.56%	93.26%	87.49%	81.98%

summarized as: 1) Our method uses more powerful Gaussian kernels while [21] uses linear kernels; 2) Our formulation can easily incorporate more kernels while [21] only uses one kernel for each feature representation; 3) By combining RFF with the L_{21} norm, our method exploits the group sparsity as well as the complementary information among different kernels. As for 2), if more kernels are to be added into [21], a much finer grid search would be required to ensure accuracy, which leads to more time expense or even intractable situation. It is also worth noting that in [21], they have used CSF, MRI as well as PET features for reporting their results. One more conclusion can be made that the L_2 norm always outperforms the L_1 norm, which may be explained by the fact that the combined kernels carry complementary information.

To better illustrate how the multiple kernel methods work, we choose one best performed run for each method and give the kernel weights comparison in Fig. 1. As can be seen, in all the methods, kernels corresponding to the ROI feature are assigned the highest weights. In other words, they select ROI as the most discriminative feature representation, which is in accordance with the conclusion from the single-feature-based SVM classifier shown in Table III.

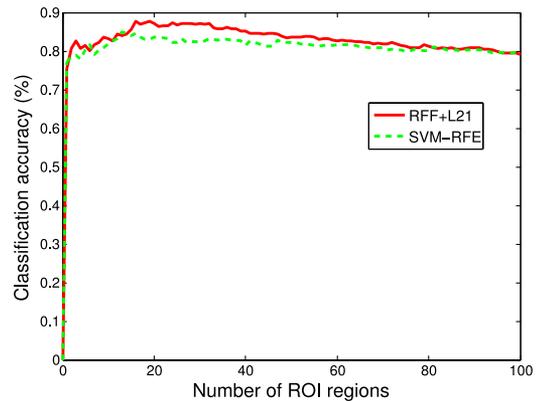


Fig. 2. Classification accuracy with respect to different number of selected ROI regions.

C. Identifying Brain Regions Closely Related to AD

In order to identify which areas of the brain region are closely related to AD, we conduct a further experiment to select the most discriminative ROI features. As mentioned previously, by imposing L_{21} norm constraint on the kernel weights, group sparsity are enforced, which actually acts as a role of feature selection. Therefore, we can treat each dimension of the ROI (each represents a certain brain region) as an individual feature to perform the RFF + L_{21} algorithm, leading to sparsity among different brain regions. More specifically, we set $p = 100$ (group size equals 1) and use $\mathbf{X}_{\text{ROI}} = \{\mathbf{x}_i^{(1)}, \mathbf{x}_i^{(2)}, \dots, \mathbf{x}_i^{(p)}\}_{i=1}^N$ as input to Algorithm 2, and then rank the regions according to the corresponding kernel weights.

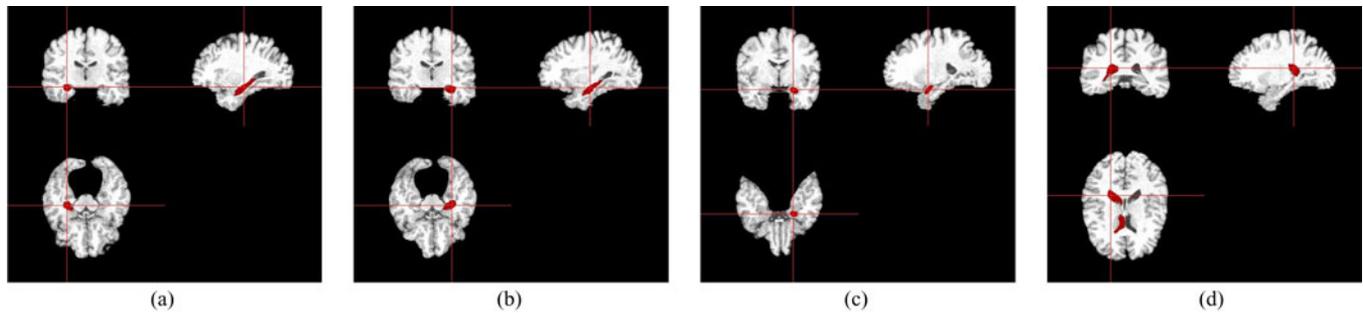


Fig. 3. Four representative brain regions selected by the proposed RFF + L_{21} method. (a) hippocampal formation right; (b) hippocampal formation left; (c) amygdala left; (d) lateral ventricle right.

TABLE V
SELECTED TOP 20 ROI REGIONS WITH THEIR CORRESPONDING AVERAGE
KERNEL WEIGHTS AND CLASSIFICATION ACCURACY

ROI region	Kernel weight	ACC (%)
hippocampal formation right	0.1364	75.62
hippocampal formation left	0.1188	80.57
occipital pole left	0.1077	82.75
uncus left	0.1077	80.68
lateral ventricle right	0.1029	81.63
fourth ventricle right	0.0803	80.25
perirhinal cortex left	0.0782	81.35
amygdala left	0.0761	82.38
lateral ventricle left	0.0517	83.75
subthalamic nucleus right	0.0493	83.37
putamen right	0.0491	82.88
inferior frontal gyrus left	0.0457	84.63
middle occipital gyrus right	0.0404	84.12
corpus callosum	0.0391	84.63
precuneus right	0.0379	85.75
medial occipitotemporal gyrus right	0.0373	88.00
nucleus accumbens left	0.0372	87.13
perirhinal cortex right	0.0362	87.62
supramarginal gyrus left	0.0355	87.87
medial occipitotemporal gyrus left	0.0327	87.25

For each dimension of the ROI features, we use three Gaussian kernels $\sigma = \{0.5, 1, 2\}$ with $C = 1$. We randomly split the dataset into 2/3 for training and 1/3 for testing and report the average performance over ten different trials. The selected top 20 regions and their average kernel weights are summarized in Table V. Note that the average kernel weights are summed over all different bandwidth kernels.

To quantitatively evaluate the effect of the feature selection, we test the classification accuracy with respect to different numbers of the selected ROI regions. For a comparison, we also implement an SVM Recursive Feature Elimination method described in [35], referred as SVM-RFE, which is a popular feature selection method. Then, according to the feature rankings, we use an increasing number of ROI features to train a Gaussian SVM with bandwidth $\sigma = \sqrt{d}$ (d is the number of ROI features) and $C = 1$. The evaluation is averaged over 20 different runs using 2/3 for training and 1/3 for testing. Fig. 2 shows the results. As can be seen, using features selected by our method is similar but statistically better than SVM-RFE. Moreover, the classification accuracy of the proposed RFF + L_{21} reaches its peak at the number of 16, and better than using all the ROI regions. We further calculate the pairwise correlations of the

top 16 features selected by each method and get the average correlation coefficients of 0.3212 and 0.3661 for RFF + L_{21} and SVM-RFE, respectively. This explains the performance in Fig. 2, as the features selected by SVM-RFE are more correlated than those selected by RFF + L_{21} . Inspired from this, we use the top 16 ranked ROI regions to reproduce the first experiment and get an accuracy of $90.75\% \pm 3.25$, even better than the one ($87.12\% \pm 3.37$) we reported in Table III. This further demonstrates the efficacy of the feature selection using the proposed method.

From Fig. 2, we can further identify the most discriminative features among the top 20. We list the classification accuracy of the top 20 regions in Table V. By selecting the one which significantly increases the accuracy according to the curve in Fig. 2, we highlight the potential regions closely related to AD in bold. Among them, “hippocampal formation right,” “hippocampal formation left,” “amygdala left,” “precuneus right,” “lateral ventricle right,” “medial occipitotemporal gyrus” are commonly known to be related to AD by many studies in the literature [36]–[38]. As examples, hippocampus, a brain area closely related to the memory, is especially vulnerable and always affected in the occurrence of AD [36]; in [38], agymdala atrophy was claimed comparable to hippocampal atrophy in AD patients; precuneus atrophy was observed in early onset of AD in [37]. Fig. 3 visualizes four examples of the selected regions (in red) against the atlas MRI with cerebellum removed.

IV. CONCLUSION

We have proposed a general yet simple MKL framework for the AD classification problem by combining multimodal features. Instead of solving the problem in the dual space as one commonly does, we propose to explicitly compute the mapping function through Fourier transform and random sampling, leading to the primal solution of the problem. The proposed method is easy to implement and scales as the linear time of the sample size. Also, we impose group Lasso constraint on the kernel weights, to enhance group sparsity among different feature representations, which selects the most discriminative feature groups, while at the same time exploiting the complementary information among different kernels within a group. Experimental results on the AD dataset demonstrate that the proposed RFF + L_{21} norm algorithm outperforms other feature fusion methods. We further utilize the feature selection of the

proposed framework to extract the most discriminative ROI features, hence identifying brain regions that most related to AD. Conclusions are in accordance with studies in the literature.

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REFERENCES

- [1] J. Ye, T. Wu, J. Li, and K. Chen, "Machine learning approaches for the neuroimaging study of Alzheimer's disease," *IEEE Comput.*, vol. 44, no. 4, pp. 99–101, Apr. 2011.
- [2] ADNI. (2011). "Alzheimer disease neuroimaging initiative," [Online]. Available: <http://adni.loni.ucla.edu/>
- [3] G. B. Frisoni, N. C. Fox, C. R. Jack, P. Scheltens, and P. M. Thompson, "The clinical use of structural MRI in Alzheimer disease," *Nat. Rev. Neurol.*, vol. 6, pp. 67–77, 2010.
- [4] A. M. Fjell, K. B. Walhovd, C. Fennema-Notestine, L. K. McEvoy, D. J. Hagler, D. Holland, J. B. Brewer, A. M. Dale, and A. D. N. Initiative, "CSF biomarkers in prediction of cerebral and clinical change in mild cognitive impairment and Alzheimer's disease," *J. Neurosci.*, vol. 30, pp. 2088–2101, 2010.
- [5] P. NL, "Reaching the limits of genome-wide significance in Alzheimer disease: Back to the environment," *J. Amer. Med. Assoc.*, vol. 303, pp. 1864–1865, 2010.
- [6] R. Casanova, C. T. Whitlow, B. Wagner, J. Williamson, S. A. Shumaker, J. A. Maldjian, and M. A. Espeland, "High dimensional classification of structural MRI Alzheimer's disease data based on large scale regularization," *Front Neuroinform.*, vol. 5, p. 22, 2011.
- [7] E. E. Tripoliti, D. I. Fotiadis, and M. Argyropoulou, "A supervised method to assist the diagnosis and monitor progression of Alzheimer's disease using data from an fMRI experiment," *Artif. Intell. Med.*, vol. 53, pp. 35–45, 2011.
- [8] S. Klöppel, C. M. Stonnington, C. Chu, B. Draganski, R. I. Scahill, J. D. Rohrer, N. C. Fox, C. R. Jack, Jr., J. Ashburner, and R. S. J. Frackowiak, "Automatic classification of MR scans in Alzheimer's disease," *Brain*, vol. 131, pp. 681–689, 2008.
- [9] Y. Fan, S. M. Resnick, X. Wu, and C. Davatzikos, "Structural and functional biomarkers of prodromal Alzheimer's disease: A high-dimensional pattern classification study," *Neuroimage*, vol. 41, pp. 277–285, 2008.
- [10] K.-K. Shen, J. Fripp, F. Meriaudeau, G. Chetelat, O. Salvado, and P. Bourgeat, "Detecting global and local hippocampal shape changes in Alzheimer's disease using statistical shape models," *NeuroImage*, vol. 59, pp. 2155–2166, 2012.
- [11] Z. Dai, C. Yan, Z. Wang, J. Wang, M. Xia, K. Li, and Y. He, "Discriminative analysis of early Alzheimer's disease using multi-modal imaging and multi-level characterization with multi-classifier," *Neuroimage*, vol. 59, pp. 2187–2195, 2012.
- [12] R. Polikar, C. Tilley, B. Hillis, and C. M. Clark, "Multimodal EEG, MRI and PET data fusion for Alzheimer's disease diagnosis," in *Proc. IEEE Annu. Int. Conf. Eng. Med. Biol. Soc.*, 2010, pp. 6058–6061.
- [13] C. Hinrichs, V. Singh, L. Mukherjee, G. Xu, M. K. Chung, S. C. Johnson, and A. D. N. Initiative, "Spatially augmented LPboosting for AD classification with evaluations on the ADNI dataset," *Neuroimage*, vol. 48, pp. 138–149, 2009.
- [14] K. B. Walhovd, A. M. Fjell, J. Brewer, L. K. McEvoy, C. Fennema-Notestine, D. Hagler, Jr., R. G. Jennings, D. Karow, A. M. Dale, and A. D. N. Initiative, "Combining MR imaging, positron-emission tomography, and CSF biomarkers in the diagnosis and prognosis of Alzheimer disease," *Amer. J. Neuroradiol.*, vol. 31, pp. 347–354, 2010.
- [15] G. R. Lanckriet, T. De Bie, N. Cristianini, M. I. Jordan, and W. S. Noble, "A statistical framework for genomic data fusion," *Bioinformatics*, vol. 20, pp. 2626–2635, 2004.
- [16] S. Sonnenberg, G. Rätsch, C. Schäfer, and B. Schölkopf, "Large scale multiple kernel learning," *J. Mach. Learn. Res.*, vol. 7, pp. 1531–1565, 2006.
- [17] G. R. Lanckriet, M. Deng, N. Cristianini, M. I. Jordan, and W. S. Noble, "Kernel-based data fusion and its application to protein function prediction in yeast," *Pacific Symp. Biocomput.*, pp. 300–311, 2004.
- [18] C. Hinrichs, V. Singh, G. Xu, and S. Johnson, "MKL for robust multi-modality AD classification," *Med. Image Comput. Comput.-Assist. Interv.*, vol. 12, pp. 786–794, 2009.
- [19] A. Rakotomamonjy, F. R. Bach, S. Canu, and Y. Grandvalet, "SimpleMKL," *J. Mach. Learn. Res.*, vol. 9, pp. 2491–2521, 2008.
- [20] R. Cuingnet, E. Gerardin, J. Tessieras, G. Auzias, S. Lehericy, M. O. Habert, M. Chupin, H. Benali, and O. Colliot, "Automatic classification of patients with Alzheimer's disease from structural MRI: A comparison of ten methods using the ADNI database," *NeuroImage*, vol. 56, pp. 766–781, 2011.
- [21] D. Zhang, Y. Wang, L. Zhou, H. Yuan, D. Shen, and A. D. N. Initiative, "Multimodal classification of Alzheimer's disease and mild cognitive impairment," *Neuroimage*, vol. 55, pp. 856–867, 2011.
- [22] L. Duan, I. W. Tsang, and D. Xu, "Domain transfer multiple kernel learning," *IEEE Trans. Pattern Anal. Mach. Intell.*, vol. 34, no. 3, pp. 465–479, Mar. 2012.
- [23] A. Rahimi and B. Recht, "Random features for large-scale kernel machines," presented at the 21st Annu. Conf. Adv. Neural Inf. Process. Syst., Vancouver, BC, Canada, 2007.
- [24] C. Cortes and V. Vapnik, "Support-vector networks," *J. Mach. Learn.*, vol. 20, pp. 273–297, 1995.
- [25] S. Boyd and L. Vandenberghe, *Convex Optimization*. Cambridge, U.K.: Cambridge Univ. Press, 2004.
- [26] Mosek, "The MOSEK interior point optimizer," (2011). [Online]. Available: <http://www.mosek.com>
- [27] F. Yan, K. Mikolajczyk, J. Kittler, and M. Tahir, "A comparison of 11 norm and 12 norm multiple kernel SVMs in image and video classification," in *Proc. Int. Workshop Content Based Multimedia Index.*, 2009, pp. 7–12.
- [28] F. R. Bach, "Consistency of the group lasso and multiple kernel learning," *J. Mach. Learn. Res.*, vol. 9, pp. 1179–1225, 2008.
- [29] Z. Xu, R. Jin, H. Yang, I. King, and M. R. Lyu, "Simple and efficient multiple kernel learning by group lasso," presented at the 27th Int. Conf. Mach. Learn., Haifa, Israel, 2010.
- [30] M. Kazhdan, T. Funkhouser, and S. Rusinkiewicz, "Rotation invariant spherical harmonic representation of 3D shape descriptors," in *Proc. Eurographics/ACM SIGGRAPH Symp. Geometry Process.*, 2003, pp. 156–164.
- [31] D. Shen, "Very High-Resolution morphometry using Mass-Preserving deformations and HAMMER elastic registration," *NeuroImage*, vol. 18, pp. 28–41, 2003.
- [32] N. Kabani, D. MacDonald, C. Holmes, and A. Evans, "A 3D atlas of the human brain," *Neuroimage*, vol. 7, pp. S717–S720, 1998.
- [33] B. W. Matthews, "Comparison of the predicted and observed secondary structure of T4 phage lysozyme," *Biochim. Biophys. Acta*, vol. 405, pp. 442–451, 1975.
- [34] C.-C. Chang and C.-J. Lin, "LIBSVM: A library for support vector machines," *ACM Trans. Intell. Syst. Technol.*, vol. 2, pp. 27:1–27:27, 2011.
- [35] I. Guyon, J. Weston, S. Barnhill, and V. Vapnik, "Gene selection for cancer classification using support vector machines," *J. Mach. Learn.*, vol. 46, pp. 389–422, 2002.
- [36] C. Misra, Y. Fan, and C. Davatzikos, "Baseline and longitudinal patterns of brain atrophy in MCI patients, and their use in prediction of short-term conversion to AD: Results from ADNI," *NeuroImage*, vol. 44, pp. 1415–1422, 2009.
- [37] G. Karas, P. Scheltens, S. Rombouts, R. van Schijndel, M. Klein, B. Jones, W. van der Flier, H. Vrenken, and F. Barkhof, "Precuneus atrophy in early-onset Alzheimer's disease: A morphometric structural MRI study," *Neuroradiology*, vol. 49, pp. 967–976, 2007.
- [38] S. Poulin, R. Dautoff, J. Morris, L. Barrett, and B. Dickerson, "Amygdala atrophy is prominent in early Alzheimer's disease and relates to symptom severity," *Psychiatry Res.*, vol. 194, pp. 7–13, 2011.

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